## IN THE CLAIMS:

1. (original) A method comprising the steps of:

when a local temperature change takes place in a certain position inside an object, acquiring a measured phase distribution image representing a temperature distribution inside said object using, as a temperature indicator, a phase of complex magnetic resonance signals from water protons inside said object observed by a magnetic resonance tomographic imaging technique;

defining a certain position in said acquired measured phase distribution image as a region of interest;

estimating a phase distribution of complex magnetic resonance signals before a temperature change in said region of interest based on a phase distribution of complex magnetic resonance signals in a portion surrounding said region of interest;

acquiring an estimated phase distribution image based on said estimated phase distribution;

calculating an amount of phase variation of complex magnetic resonance signals caused by a temperature change in said region of interest by conducting subtraction between said measured phase distribution image and said estimated phase distribution image on a pixel-by-pixel basis; and

measuring an amount of a temperature change in said region of interest based on said amount of variation.

2. (original) A method comprising the steps of:

when a local temperature change takes place in a certain position inside an object, acquiring a real-part image and an imaginary-part image as measured complex images incorporating a temperature distribution inside said object using, as a temperature indicator, a phase of complex magnetic resonance signals from water protons inside said object observed by a magnetic resonance tomographic imaging technique;

defining the same position in said acquired real-part and imaginary-part images as a region of interest;

estimating a distribution of a real part and an imaginary part of complex magnetic resonance signals before a temperature change in said region of interest based on a distribution of a real part and an imaginary part of complex magnetic resonance signals in a portion surrounding said region of interest;

acquiring an estimated complex image based on said estimated real-part and imaginary-part distribution;

calculating an amount of phase variation of complex magnetic resonance signals caused by a temperature change in said region of interest by calculating a phase difference between said measured complex image and said estimated complex image on a pixel-by-pixel basis; and

measuring an amount of a temperature change in said region of interest based on said amount of variation.

3. (original) The method as defined by claim 1, characterized in comprising: estimating a phase distribution of complex magnetic resonance signals in a region of interest by applying higher-order rational polynomial fitting by a linear least squares method, functional fitting by a non-linear least squares method, or a finite element method to a phase

distribution of complex magnetic resonance signals in a portion surrounding said region of interest.

- 4. (original) The method as defined by claim 2, characterized in comprising: estimating a distribution of a real part and an imaginary part of complex magnetic resonance signals in a region of interest by applying higher-order rational polynomial fitting by a linear least squares method, functional fitting by a non-linear least squares method, or a finite element method to a distribution of a real part and an imaginary part of complex magnetic resonance signals in a portion surrounding said region of interest.
- 5. (currently amended) The method as defined by elaim 1 or 3 claim 1, characterized in comprising: conducting subtraction between a measured phase distribution image and an estimated phase distribution image on a pixel-by-pixel basis by multiplying complex conjugates of complex numbers of complex magnetic resonance signals with each other and calculating an arctangent of the product.
- 6. (currently amended) The method as defined by elaim 2 or 4 claim 2, characterized in comprising: calculating a phase difference between a measured complex image and an estimated complex image on a pixel-by-pixel basis by multiplying complex conjugates of complex numbers of complex magnetic resonance signals with each other and calculating an arctangent of a ratio between a real part and an imaginary part of the product.
- 7. (currently amended) The method as defined by any one of claims 1 6 claim 1, characterized in comprising: outputting a distribution image of the amount of a temperature change based on the amount of phase variation of complex magnetic resonance signals superimposed over an anatomical image of organ or tissue acquired by a magnetic resonance tomographic imaging technique.
- 8. (currently amended) The method as defined by any one of claims 1 7 claim 1, characterized in comprising: capturing a phase distribution image of complex

magnetic resonance signals in one, two or three orthogonal planes intersecting an extension of an in-body penetrating portion of a heating or cooling apparatus during thermo-treatment or cryo-treatment so as to include a tip of said in-body penetrating portion, or in two or more parallel planes.

- 9. (original) The method as defined by claim 8, characterized in comprising: checking the position of the tip of the in-body penetrating portion of the heating or cooling apparatus using an optical positioning apparatus, and capturing a phase distribution image of complex magnetic resonance signals so as to include said tip.
- 10. (original) The method as defined by claim 9, characterized in comprising: providing a marker at the tip of said in-body penetrating portion, and checking a position of the tip of said in-body penetrating portion by detecting said marker in an MRI image or numerically detecting it.
- 11. (original) The method as defined by claim 10, wherein: the method of providing the marker comprises providing the tip of said in-body penetrating portion with inductor elements or applying a contrast agent to the tip of said in-body penetrating portion.
- 12. (currently amended) The method as defined by any one of claims 8—11 claim 8, characterized in comprising: when target organ or tissue moves with body motion, capturing a phase image of complex magnetic resonance signals following the movement or covering a range of the movement.
  - 13. (original) A temperature change measurement apparatus comprising:

means of, when a local temperature change takes place in a certain position inside an object, producing a measured phase distribution image representing a temperature distribution of said object using, as a temperature indicator, a phase of complex magnetic

resonance signals from water protons inside said object observed by a magnetic resonance tomographic imaging technique;

means of defining a region of interest in said acquired measured phase distribution image;

means of estimating a phase distribution of complex magnetic resonance signals before a temperature change in said region of interest based on a phase distribution of complex magnetic resonance signals in a portion surrounding said region of interest;

means of producing an estimated phase distribution image based on said estimated phase distribution;

means of producing a phase difference distribution image from a phase difference in complex magnetic resonance signals caused by a temperature change in said region of interest by conducting subtraction between said measured phase distribution image and said estimated phase distribution image on a pixel-by-pixel basis; and

means of calculating a temperature change from said phase difference distribution image.

## 14. (original) A temperature change measurement apparatus comprising:

means of, when a local temperature change takes place in a certain position inside an object, producing a real-part image and an imaginary-part image as measured complex images incorporating a temperature distribution of said object using, as a temperature indicator, a phase of complex magnetic resonance signals from water protons inside said object observed by a magnetic resonance tomographic imaging technique;

means of defining a region of interest in said acquired measured complex image;

means of estimating a complex image before a temperature change in said region of interest based on a distribution of a real part and an imaginary part of complex magnetic resonance signals in a portion surrounding said region of interest;

means of producing an image representing the amount of phase variation of complex magnetic resonance signals caused by a temperature change in said region of interest by calculating a phase difference between said measured complex image and said estimated complex image on a pixel-by-pixel basis; and

means of calculating a temperature change from said phase distribution image.

- 15. (original) The apparatus as defined by claim 13, characterized in that: said means of estimating a phase distribution applies higher-order rational polynomial fitting by a linear least squares method, functional fitting by a non-linear least squares method, or a finite element method to a phase distribution of complex magnetic resonance signals in a portion surrounding said region of interest.
- 16. (original) The apparatus as defined by claim 14, characterized in that: said means of estimating a phase distribution applies higher-order rational polynomial fitting by a linear least squares method, functional fitting by a non-linear least squares method, or a finite element method to a distribution of a real part and an imaginary part of complex magnetic resonance signals in a portion surrounding said region of interest.
- 17. (currently amended) The apparatus as defined by elaim 13 or 15 claim 13, characterized in that: said means of producing a phase difference distribution image conducts subtraction between a measured phase distribution image and an estimated phase distribution image on a pixel-by-pixel basis by multiplying complex conjugates of complex numbers of complex magnetic resonance signals with each other and calculating an arctangent of the product.

- 18. (currently amended) The apparatus as defined by elaim 14 or 16 claim 14, characterized in that: said means of producing a phase difference distribution image calculates a phase difference between a measured complex image and an estimated complex image on a pixel-by-pixel basis by multiplying complex conjugates of complex numbers of complex magnetic resonance signals with each other and calculating an arctangent of the ratio between a real part and an imaginary part of the product.
- 19. (currently amended) The apparatus as defined by any one of claims 13—18 claim 13, characterized in comprising: in addition to said means of producing a phase difference distribution image representing the amount of phase variation of complex magnetic resonance signals caused by a temperature change in a region of interest, means of outputting a temperature image calculated from said phase difference distribution image superimposed over an anatomical image of organ or tissue.
- 20. (currently amended) The apparatus as defined by any one of claims 13—19 claim 13, characterized in comprising: to capture a measured phase distribution image or measured complex image, means of checking a tip of an in-body penetrating portion of a heating or cooling apparatus, and capturing a phase distribution image or a complex image of complex magnetic resonance signals in one, two or three orthogonal planes intersecting an extension of the in-body penetrating portion of the heating or cooling apparatus, or in two or more parallel planes.
- 21. (original) The apparatus as defined by claim 20, characterized in that: a position of the tip of the in-body penetrating portion of the heating or cooling apparatus is checked using an optical positioning apparatus.
- 22. (original) The apparatus as defined by claim 21, characterized in that: a marker is provided at the tip of said in-body penetrating portion, and the position of the tip of

said in-body penetrating portion is further checked by detecting said marker by an MRI apparatus.

- 23. (original) The apparatus as defined by claim 22, characterized in that: said means of providing a marker provides the tip of said in-body penetrating portion with inductor elements or applies a contrast agent to the tip of said in-body penetrating portion.
- 24. (currently amended) The apparatus as defined by any one of claims 21 23 claim 21, characterized in that: when target organ or tissue moves with body motion, the position of the tip of the in-body penetrating portion of the heating or cooling apparatus is checked following the movement or covering a range of the movement.
- 25. (new) The method as defined by claim 2, characterized in comprising: outputting a distribution image of the amount of a temperature change based on the amount of phase variation of complex magnetic resonance signals superimposed over an anatomical image of organ or tissue acquired by a magnetic resonance tomographic imaging technique.
- 26. (new) The method as defined by claim 2, characterized in comprising: capturing a phase distribution image of complex magnetic resonance signals in one, two or three orthogonal planes intersecting an extension of an in-body penetrating portion of a heating or cooling apparatus during thermo-treatment or cryo-treatment so as to include a tip of said in-body penetrating portion, or in two or more parallel planes.
- 27. (new) The method as defined by claim 26, characterized in comprising: checking the position of the tip of the in-body penetrating portion of the heating or cooling apparatus using an optical positioning apparatus, and capturing a phase distribution image of complex magnetic resonance signals so as to include said tip.
- 28. (new) The method as defined by claim 27, characterized in comprising: providing a marker at the tip of said in-body penetrating portion, and checking a position of

the tip of said in-body penetrating portion by detecting said marker in an MRI image or numerically detecting it.

- 29. (new) The method as defined by claim 28, wherein: the method of providing the marker comprises providing the tip of said in-body penetrating portion with inductor elements or applying a contrast agent to the tip of said in-body penetrating portion.
- 30. (new) The method as defined by any one of claim 26, characterized in comprising: when target organ or tissue moves with body motion, capturing a phase image of complex magnetic resonance signals following the movement or covering a range of the movement.
- 31. (new) The apparatus as defined by claim 14, characterized in comprising: in addition to said means of producing a phase difference distribution image representing the amount of phase variation of complex magnetic resonance signals caused by a temperature change in a region of interest, means of outputting a temperature image calculated from said phase difference distribution image superimposed over an anatomical image of organ or tissue.
- 32. (new) The apparatus as defined by claim 14, characterized in comprising: to capture a measured phase distribution image or measured complex image, means of checking a tip of an in-body penetrating portion of a heating or cooling apparatus, and capturing a phase distribution image or a complex image of complex magnetic resonance signals in one, two or three orthogonal planes intersecting an extension of the in-body penetrating portion of the heating or cooling apparatus, or in two or more parallel planes.
- 33. (new) The apparatus as defined by claim 32, characterized in that: a position of the tip of the in-body penetrating portion of the heating or cooling apparatus is checked using an optical positioning apparatus.

- 34. (new) The apparatus as defined by claim 33, characterized in that: a marker is provided at the tip of said in-body penetrating portion, and the position of the tip of said in-body penetrating portion is further checked by detecting said marker by an MRI apparatus.
- 35. (new) The apparatus as defined by claim 34, characterized in that: said means of providing a marker provides the tip of said in-body penetrating portion with inductor elements or applies a contrast agent to the tip of said in-body penetrating portion.
- 36. (new) The apparatus as defined by claim 33, characterized in that: when target organ or tissue moves with body motion, the position of the tip of the in-body penetrating portion of the heating or cooling apparatus is checked following the movement or covering a range of the movement.